A Universal Fast Colorimetric Method for DNA Signal Detection with DNA Strand Displacement and Gold Nanoparticles

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DNA or gene signal detection is of great significance in many fields including medical examination, intracellular molecular monitoring, and gene disease signal diagnosis, but detection of DNA or gene signals in a low concentration with instant visual results remains a challenge. In this work, a universal fast and visual colorimetric detection method for DNA signals is proposed. Specifically, a DNA signal amplification “circuit” based on DNA strand displacement is firstly designed to amplify the target DNA signals, and then thiol modified hairpin DNA strands and gold nanoparticles are used to make signal detection results visualized in a colorimetric manner. If the target DNA signal exists, the gold nanoparticles aggregate and settle down with color changing from dark red to grey quickly; otherwise, the gold nanoparticles’ colloids remain stable in dark red. The proposed method provides a novel way to detect quickly DNA or gene signals in low concentrations with instant visual results. When applied in real-life, it may provide a universal colorimetric method for gene disease signal diagnosis.

1. Introduction

Biocomputing refers to the field of exploiting biological macromolecules or organisms to implement relatively standard methods of computation [1–5]. In recent years, computing with programmable DNA molecules has become a promising research topic, and lots of pioneering conceptual works contributed to the field, such as helical molecular programming approach [6], DNA self-assembly for computation [7, 8], molecular computing methods to improve the accuracy of insertion site analysis in tumors [9], and tabletop molecular communications with chemical signals [10]. One of the widely used technologies in DNA programming is DNA strand displacement [11].

DNA strand displacement technology was proposed as an in vitro isothermal and enzyme-free DNA amplification technique [11, 12]. During the past decades, it has become a popular studied branch of DNA programming. The most notable merit of DNA strand displacement is that during its process all DNA strands interact with one another automatically and cannot “cross talk” with other unrelated strands by “carefully” sequence design. The technique is selective to the recognition of DNA sequence [13] and has been used to detect DNA signals [14–19]. With DNA strand displacement, some biomolecular signal processing systems have been developed, such as enzyme-free nucleic acid logic circuits [20], genetic programming and evolvable molecular machines [21], performing logic computation of Hopfield network autoassociative memory with DNA strands [22], kinetically controlled self-assembly of DNA oligomers [23], and logic gates with “DNA neurons” [24].

A DNA molecular system seems to be functioning unit with DNA strands having particular biological functions. In the system, information is encoded and stored in form of DNA strands, and each of DNA strands performs its own reactions independently. The output DNA strands in certain reaction can be taken as input of other reactions, which in some sense can process information like functioning
DNA strands are represented by straight lines with arrows that denote the direction from 5' to 3', as shown in Figure 1. A specific segment of oligonucleotides is defined as a "domain" to make clear the comprehension of DNA hybridization, branch migration, and dissociation. Each domain is represented by a straight line of specific color and length, such as domains S1, S2, T, T’, S6, S6’, and C in Figure 1.

The domains labeled with the letter “S” are "recognition domains," and the ones with label “T” or “C” are the “toehold domains.” For any domain α, we use α’ to represent its complementary domain, where α can be the label of any domain. For example, domain S6 is complementary with domain S6’. In DNA signal amplification “circuit,” there are four main types of strands, that is, “Input,” “Output,” “Gate,” and “Fuel.” DNA signal amplification “circuit” is based on the principle of toehold-mediated DNA strand displacement. It starts from a single-stranded DNA binding to the uncovered toehold domain by its own toehold domain and then allowing the migration of the prehybridized recognition domain and adhesion of incoming recognition domain. With the “circuit,” the single-stranded DNA strand (DNA signal) can be replaced by the quondam bound single-stranded DNA; see [32, 33]. There are two reactions in DNA signal amplification "circuit."

One reaction is the seesawing reaction, whose schematic diagram is shown in Figure 2.

This reaction happens when “Input” strands talk with “Gate” strands adhering to the Input-Gate complex. Initially, “Input” strand hybridizes to the extended toehold domain of “Gate” strand (T’ domain on the rightmost), and domain S6 of “Input” strand squeezes out that of “Gate” complex such that “Output” strand will be released and Input-Gate complex is produced at the same time. After Input-Gate complex is produced, “Fuel” strand will hybridize to the uncovered toehold domain of the Input-Gate complex and release “Input” strand again and “Waste” strands. With the reaction, it forms a catalytic cycle, by which “Fuel” strand can be consumed with producing “Output” strand, while the amount of “Input” strands keeps changeless. In this way, “Output” strand can be produced with consumption of “Fuel” strands, but without any reduction of “Input” strands.

2. Methods

In this section, we introduce the structure of DNA signal amplification “circuit” with DNA strand displacement, and then the visualized colorimetric method for DNA signal (in a low concentration) detection is described in detail.

2.1. DNA Signal Amplification "Circuit". It starts by introducing the way to represent DNA strands, and then the basic reactions used in DNA signal amplification “circuit” are introduced.
The second reaction, that is, the reporting reaction, takes place if and only if “Output” strand has been released in seesawing reaction. When “Output” strand is released, it will adhere to the “Reporter” complex via its toehold, starting the migration and displacement. Domain $S_1$ of “Output” strand will hybridize with domain $S_1'$ of “Reporter” strand. In this way, hairpin structure of “Reporter” strand will be forced to unfold producing the Output-Report complex, which is the resulting strand by amplifying “Input” strands.

With the two basic reactions, DNA signal amplification “circuit” can be built as shown in Figure 3. When target DNA signal “Input” strand is present, a seesawing reaction occurs immediately to release “Output” strand; meanwhile, “Fuel” strand hybridizes to the intermediary complex (Input-Gate complex) to release “Input” strands and the “Waste” strands. In this way, the “Input” strand can be produced as soon as it is consumed, so the seesawing reaction does not reduce the amount of “Input” strand. It is noted that the volume of “Fuel” strand should be several times as much as that of “Input” strand, which will promote seesawing reaction circle towards the direction of producing “Outputs” strand. If no “Input” strand is added to “circuit,” then no “Output” strand can be released.

2.2. The Visualized Colorimetric DNA Signal Detection Method. It is known that gold nanoparticles could aggregate and precipitate in a solution of high concentration [34–39]. If gold nanoparticles cannot be connected with DNA through thiol group, they will aggregate and settle down with color changing from dark red to grey with adding salt solution; otherwise, they remain stable and in color dark red. With this fact, we develop a visualized colorimetric DNA signal detection method with aggregation and precipitation of gold nanoparticles.

A “Reporter” strand (see Figure 4) is hereby designed, whose 5' side is connected with a thiol group. The schematic diagram of the visualized colorimetric DNA signal detection method is depicted in Figure 5.

If “Output” strand cannot be produced, which means no target “Input” strand exists, then thiol group of “Reporter” will bind to gold nanoparticles to prevent them from aggregating. In this case, gold nanoparticles will remain stable in dark red. The schematic diagram of the process is given in Figure 5(a).

If “Output” strand can be produced, which means target “Input” strand exists, then the thiol group of “Reporter” will
Table 1: Sequences and domains with all sequences starting from 5’ end to 3’ end.

<table>
<thead>
<tr>
<th>Primer</th>
<th>Domains</th>
<th>Sequence</th>
</tr>
</thead>
<tbody>
<tr>
<td>P1</td>
<td>S6 + T + S2</td>
<td>CATAACACAATCACA + TCT + CAAAACAAAAACCTCA</td>
</tr>
<tr>
<td>P2</td>
<td>S7 + T + S6</td>
<td>CAACATATCATACTCA + TCT + CATAACACAATCACA</td>
</tr>
<tr>
<td>P3</td>
<td>T’ + S6’ + T’</td>
<td>AGA + TGTGATTGTGTTATG + AGA</td>
</tr>
<tr>
<td>P4</td>
<td>S1 + T + S6</td>
<td>CATCCATTCCACTCA + TCT + CATAACACAATCACA</td>
</tr>
<tr>
<td>P5</td>
<td>C’ + T’ + S1’ + S1</td>
<td>TG + AGATGA + GTGGAATGGATG + TTTTTTTTTTTTTT + CATCCATTCCACTCA</td>
</tr>
</tbody>
</table>

Table 2: Components of “Input,” “Output,” “Gate,” and “Fuel.”

<table>
<thead>
<tr>
<th>ID</th>
<th>Formation</th>
<th>Function</th>
<th>Concentration</th>
</tr>
</thead>
<tbody>
<tr>
<td>C1</td>
<td>P1</td>
<td>Input</td>
<td>5 μM</td>
</tr>
<tr>
<td>C2</td>
<td>P2</td>
<td>Fuel</td>
<td>5 μM</td>
</tr>
<tr>
<td>C3</td>
<td>P3, P4</td>
<td>Gate</td>
<td>5 μM</td>
</tr>
<tr>
<td>C4</td>
<td>P5</td>
<td>Output</td>
<td>10 μM</td>
</tr>
</tbody>
</table>

Figure 4: The schematic diagram of reporting reaction.

3. Experimental Results

3.1. Materials

3.1.1. DNA Strands Preparation. All DNA strands were acquired from Shanghai Sangon Co. Ltd. Disulfide functionalized DNA strands were purified through high-performance liquid chromatography (HPLC). Unmodified DNA strands were also purified through HPLC. After being chemically synthesized and shipped as powder, DNA oligonucleotides were suspended in Milli-Q water (Millipore) and stored at 4°C at ~100 μM. The sequences of the oligonucleotides are listed in Table 1 for ease of reference. Besides, HAuCl₄·3H₂O, trisodium citrate, and sodium chloride were also purchased from Shanghai Sangon Co. Ltd.

3.1.2. Gold Nanoparticles Preparation. Gold nanoparticles were prepared by the citrate reduction of HAuCl₄. 100 mL ultrapure water, 2 mL auric chloride acid (0.5%), and 10 mL trisodium citrate (1%) are added to 250 mL conical flask and shook up. The mixture is heated with high heat in microwave oven for 1 minute and with medium heat for 5 minutes. Finally the gold nanoparticles colloids is cooled down at room temperature and examined by TEM (Transmission Electron Microscope). The obtained picture is shown in Figure 6. The TEM result shows that gold nanoparticles spread evenly with ~20 nm diameters.

3.1.3. Amplification “Circuit” Formation. In the DNA signal amplification “circuit,” there are four kinds of strands “Input,” “Output,” “Gate,” and “Fuel.” Their formations and concentrations are shown in Table 2. The “Gate” is formed in a course of slow annealing. All the components are stored at 4°C.

3.2. Experimental Observations. The scheme of DNA signal amplification and colorimetric detection of gold nanoparticles is shown in Figure 7. There are two test tubes in DNA signal amplification reaction, which are labeled by T1 and T2, respectively; see Figure 7(a). DNA signal amplification “circuit” is constructed with 5 μL “Gate” and 5 μL “Fuel” and put into each of test tubes T1 and T2.

1 μL target DNA signal “Input” strand is added to T2, while the same amount of ultrapure water is added to T1 for comparison (see Figure 7(a)). Disulfide functionalized “Reporter” is added to both of two test tubes 0.5 hour later. Tubes TA and TB (with gold nanoparticles colloids) are kept.
for 22 hours for sufficient attachment between thiol groups and gold nanoparticles. After 0.5 hour, we add 3 μL solution from tube T1 to TA and add 3 μL solution from tube T2 to TB, where tubes TA and TB are with 20 μL gold nanoparticles colloid (see Figure 7(b)). Eventually, 0.5 μL salt solution is added to each of tubes TA and TB.

The results of signal amplification of native PAGE (polyacrylamide gel electrophoresis) and visible detection results are shown in Figure 8.

In Figure 8(a), PAGE results of DNA signal amplification “circuit” are given. From the first line to the fourth, it indicates admixture of “Reporter” and “Output,” “Reporter,” amplification “circuit” without “Input,” and amplification “circuit” with “Input,” respectively. The PAGE results of admixture of “Reporter” and “Output,” “Reporter,” and “Reporter” capped with thiol group are shown in Figure 8(b). Thiol group functionalized “Reporter” is added to detect the “Output” strand. It is shown in Figure 8(c) that solution in tube A is in color dark red (indicating that no target “Input” strand exists); solution in tube B is in color grey (indicating that
target “Input” strand exists). The detection result can be easily visualized.

Gold nanoparticles spreading status is examined by TEM. The UV-Vis absorption spectra of the sample are detected by the spectra photo meter K5500 with sample diameter of 1.0 mm and 0.2 mm. The UV-Vis absorption spectra of 20 nm pure gold nanoparticles with sampled diameters 1.0 mm (blue) and 0.2 mm (red) are shown in Figure 9.

Similarly, gold nanoparticles in tubes TB with target DNA signal and TA without target DNA signal are examined by TEM, and the UV-Vis absorption spectra of these samples are detected by the spectra photo meter K5500 with sample diameter of 1.0 mm and 0.2 mm, respectively. The TEM pictures and UV-Vis absorption spectra of 20 nm gold nanoparticles in tube TA and TB are shown in Figures 10 and 11.

The TEM result of pure gold nanoparticles shown in Figure 9 indicates that the diameter of gold nanoparticle spread evenly around 20 nm, and the UV-Vis absorption spectra result show absorption peak around 520 nm. The TEM result of tube TA shown in Figure 10 indicates if no “Input” strand (target DNA signal) exists, gold nanoparticles cannot aggregate and settle down with 0.5 M NaCl added in the solution, and UV-Vis peak around 520 nm can be observed. The TEM result of tube TB is shown in Figure 11, which indicates if “Input” strand (target DNA signal) exists, it can be amplified by the amplification “circuit” and gold nanoparticles will aggregate and settle down with 0.5 M NaCl added in the solution, color changing from dark red to grey. The correspondence UV-Vis absorption spectra results show no absorption peak around 520 nm which confirmed the aggregation of gold nanoparticles.

3.3. Discussion. In this work, we propose a method for detection of DNA signals, where the detection results can be visualized in a colorimetric manner. Specifically, a DNA signal amplification “circuit” based on DNA strand displacement is firstly designed to amplify the target DNA signals, and then thiol modified hairpin DNA strands and gold nanoparticles are used to make signal detection results visualized in a colorimetric manner. PAGE results shown in Figures 8(a) and 8(b) indicate good performances of the DNA signal amplification “circuit,” as well as the detection results which can be visualized by the color (dark red or grey) of solution induced by aggregation or not of gold nanoparticles. We
investigate the stability of the proposed method by repeating the experiment 5 times. In each experiment, we can observe the color changing as theoretically designed and can achieve the similar TEM images of gold nanoparticles and UV-Vis spectra. With this fact, it is believed that our method should be stable.

Although DNA strand displacement performs well in detecting DNA signal, there are still some problems for further research. One is the leaky reaction, in which “Output” strand can be produced even if no “Input” strand is present. Leaky reaction may cause serious consequences and could lead to logic errors [40–42]. In our method, we ameliorate the DNA strand displacement reaction by tailoring its reaction time and reducing the volume of fuel strand. Furthermore, the concentration of gate complex is selected to be 5μM in our experiment with the purpose to give a palpable result and coordinate an appropriate rate between DNA and gold nanoparticles. The volume can be further reduced to
nM-scale to improve the sensitivity of detection enormously, since the volume of “Output” is closely related to the volume of “Gate” rather than that of “Input” strand. In this way, from the theoretical point of view, even a single “Input” strand can be detected using our strategy, but we do not verify it in the present work.

Compared to Storhoff’s colorimetric DNA detection method with gold nanoparticle, our method has the merits of fluorescence-free and enzyme-free, which undergo a color change that is visually detectable [36]. Also, DNA signal amplification “circuit” with DNA strand displacement proposed in this work is more universal comparing to the formal works that nucleic acid targets are recognized by DNA-modified gold probes. This is due to the fact that in our method the target DNA signal is merely an input signal of DNA logical gate, while DNA-modified gold probes could be programmed as a constant DNA sequence with only response to the output of DNA strand displacement. Furthermore, the formal works can only deal with unamplified DNA signals, but our method has the function to DNA signal amplification.

4. Conclusion and Future Work

This paper developed a universal fast colorimetric method to detect DNA signal in low concentrations. A DNA signal amplification “circuit” with DNA strand displacement is firstly developed to magnify unsensitive and selective DNA signals, and then thiol modified hairpin DNA strands and gold nanoparticles are used to make detection results visualized in a colorimetric manner. With the DNA amplification “circuit,” target DNA signal can be amplified into a signal of certain size by DNA strand displacement, which provides great convenience to subsequent detection. Besides, process of signal amplification is independent with detection.

Both qualitative and quantitative detection are achieved. It is worthy to study what will happen if “Threshold” complex constructed in [24] is added to the “circuit.” In addition, the concentrations of components are set as μM-scale limited by properties of gold nanoparticles, but more sensitivity is attainable when concentrations are reduced.

Conflict of Interests

The authors declare that there is no conflict of interests regarding the publication of this paper.

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